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I, JULIE BILLINGSLEY, TEAM LEADER EXAMINATION SUPPORT AND SALES hereby certify that annexed is a true copy of the Provisional specification in connection with Application No. 2003906212 for a patent by SUNSHINE HEART COMPANY PTY LTD as filed on 11 November 2003.



WITNESS my hand this
Tenth day of November 2004

A handwritten signature in cursive script, reading 'J. Billingsley'.

JULIE BILLINGSLEY
TEAM LEADER EXAMINATION
SUPPORT AND SALES

AUSTRALIA

Patents Act 1990

PROVISIONAL SPECIFICATION FOR THE INVENTION ENTITLED:

Actuator for a Heart Assist Device

Name and Address of Applicant:

**Sunshine Heart Company Pty Ltd, an Australian company ACN 090 552 300, of
Unit 2, 10 Rodborough Road, Frenchs Forest, New South Wales, 2086, Australia**

Name of Inventor:

Scott Hugh Miller

This invention is best described in the following statement:

Actuator for a heart assist device

Field of the Invention

The present invention relates generally to heart assist devices, systems and methods and, more particularly, to an actuator for a counter-pulsation heart assist device.

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Background of the Invention

US Patent No. 4630597 and International PCT Patent Application No. PCT/US00/22992 (WO 01/13974) both disclose heart assist devices that utilise an inflatable balloon that is positioned within an arterial vessel of a patient. The balloons replace a resected portion of the vessel and are cyclically inflated and deflated to expand
10 into the vessel and thus assist in blood displacement during diastole and retract from within the vessel during systole.

Both of the above documents disclose devices that have a relatively rigid shell with an inlet/outlet port which is connected to a fluid pump. The flexible balloon seals around the periphery of the shell and extends back over the shell for some or all of its
15 exterior. Another layer of material is then placed over the balloon exterior, adjacent the shell, to secure the balloon to the shell.

It is an object of the present invention to provide an improved blood displacing device.

Summary of the Invention

20 Accordingly, in a first aspect, the present invention provides an actuator for a heart assist device, the actuator including:

an inflatable balloon having a first body portion, a second body portion and a flexure region joining the first and second body portions; and

25 a shroud or wrap adjacent the first body portion and having a peripheral extent at least equal to the peripheral extent of the balloon flexure region;

wherein the balloon and the shroud or wrap are shaped such that the shroud or wrap restrains a part of the balloon first body portion at or near the flexure region against displacement towards the shroud or wrap (outward displacement) past a predetermined limit but allows unrestrained displacement away from the shroud or wrap (inward
30 displacement).

The balloon and the shroud are preferably shaped such that the shroud restrains said part of the balloon first body portion at or near the flexure flexure region against

outward displacement during inflation of the balloon but allows unrestrained inward displacement during deflation.

5 Preferably, during inward displacement, at least part of the inner surface of the balloon second body portion is able to be drawn against at least part of the inner surface of the balloon first body portion.

The shroud is preferably generally inwardly concave, most preferably elongated and elliptical.

The first body portion, second body portion and flexure region are preferably integrally formed, most preferably by dip moulding.

10 The blood displacing device preferably also includes a bushing adapted for connection to a motive power source.

The balloon preferably also includes a neck portion joined to the first portion, the neck portion being adapted for sealing connection with the bushing.

15 The shroud preferably also includes a neck portion adapted for sealing connection with the balloon neck portion.

In a second aspect, the present invention provides an actuator for a heart assist device, the actuator including:

a bushing adapted for connection to a hydraulic or pneumatic power source;

20 an inflatable balloon having a narrower neck portion adapted for sealing connection with the bushing exterior, wider first and second body portions and an arcuate flexure region joining the first and second body portions, the first body portion having a first end adjacent the neck portion and a second end adjacent the second body portion and being generally inwardly concave, the second body portion being inwardly concave when the balloon is inflated and generally outwardly concave when the balloon is deflated.

25 The device preferably also includes a shroud or wrap having a body portion with a peripheral extent at least equal to the peripheral extent of the balloon first and second body portions.

30 The balloon and the shroud or wrap are preferably shaped such that a part of the balloon first body portion at or near the flexure region is restrained against outward displacement past a predetermined limit by the shroud or wrap but unrestrained against inward displacement.

Preferably, during inward displacement, at least part of the inner surface of the balloon second body portion is able to be drawn directly against at least part of the inner surface of the balloon first body portion.

In a third aspect, the present invention provides a heart assist device including:

a hydraulic or pneumatic power source; and

an actuator including:

a bushing adapted for operative connection to the motive power source;

5 an inflatable balloon having a narrower neck portion adapted for sealing connection with the bushing exterior, wider first and second body portions and a flexure region joining the first and second body portions, the first body portion having a first end adjacent the neck portion and a second end adjacent the second body portion and being generally inwardly concave, the second body portion being generally inwardly concave when the balloon is inflated and generally outwardly concave when the balloon is deflated; and

10 a shroud or wrap having a body portion with a peripheral extent at least equal to the peripheral extent of the balloon first and second body portions,

wherein the balloon and the shroud are shaped such that a part of the
15 balloon first body portion at or near the flexure region is restrained against outward displacement by the shroud past a predetermined limit but unrestrained against inward displacement.

Preferably, during inward displacement, at least part of the inner surface of the
20 balloon second body portion is able to be drawn against at least part of the inner surface of the balloon first body portion.

Preferably, the balloon and shroud are shaped such that substantially all of the balloon first body portion is restrained against outward displacement by the shroud and unrestrained against inward displacement.

25 In its preferred form, the heart assist device is configured for extra-aortic counter-pulsation. In this form, the balloon is positioned on the exterior of an arterial vessel.

In a further form, the heart assist device is configured for use either as an interposition graft in which the device replaces a completely resected section of the aorta or as an aortic patch in which an aperture is formed in the aorta which is filled with the
30 device.

When the balloon is inflated, the flexure region preferably has a radius of curvature of at least 0.1 mm, more preferably a radius of curvature of approximately 1.0 mm and most preferably a radius of curvature of approximately 3.0 mm.

The ratio of the diameter of the balloon neck portion to the balloon flexure region is preferably no more than approximately 3:1.

The bushing preferably has an inlet/outlet bore. The bore preferably also includes one or more internal restrictions adapted to prevent suction of the balloon into the bore.

5 The balloon is preferably formed from silicone, polyurethane or a polyurethane-polysiloxane block co-polymer. The balloon is preferably formed by mandrel dipping.

The balloon is preferably formed by dipping a suitably shaped mandrel into the polymer and allowing a thin coating of the polymer to cure on the mandrel. The balloon is preferably made of 2 to 4 coatings, with a total thickness of 150-300 microns. The
10 balloon can then be removed from the mandrel.

The balloon neck portion is preferably a snug sealing fit over the bushing exterior. The shroud neck portion is preferable a snug sealing fit over the balloon neck portion.

The bushing preferably has a slightly tapered neck portion adapted for
15 engagement with the balloon neck portion. The bushing neck portion preferably has a converging taper in the direction of the balloon.

The balloon is preferably held in place on the aorta by a flexible wrap which extends about the aorta and bears against the first body portion of the balloon or a shroud mounted thereon. The wrap is preferably shaped to fit the second body portion of the
20 balloon, and if desired also the neck portion. The wrap is preferably inelastic or slightly elastic so that it's stretch and flexibility characteristics match those of the native aorta.

In a fourth aspect, the present invention provides a flexible inflatable balloon for a blood displacing heart assist device, the balloon including:

a neck portion having first and second ends;

25 a substantially annular first body portion connected at its inner periphery to the neck portion second end; and

a substantially oval or circular second body portion connected at its outer periphery to the outer periphery of the first body portion,

the outer peripheries of the first and second body portions are connected along an
30 annular inwardly concavely curved flexure portion adapted to maintain a radius of curvature during movement of the second body portion between inwardly concave and outwardly concave during deflation and inflation of the balloon respectively.

The balloon is advantageously formed as a single piece. This avoids the presence of a seam line as is disclosed in US Patent specification 4,630,597 or

International patent specification WO 01/13974. Such seam lines have been found by the present inventors to raise stress levels in the balloon and reduce the operational life of the balloon.

5 A shroud can be provided to overlie and abut the annular first body portion of the balloon. The shroud is preferably shaped such that the shroud restrains said portion of the balloon at or near the flexure region against outward displacement during inflation of the balloon but allows unrestrained inward displacement during deflation. The shroud is preferably generally inwardly concave, most preferably elongated and elliptical. The shroud preferably also includes a neck portion adapted for sealing connection with the
10 balloon neck portion.

The balloon preferably also includes a bushing adapted for connection to an hydraulic or pneumatic power source. The bushing also acts to prevent inward collapse of the balloon neck portion during deflation. If desired the bushing can be formed with internal restrictions such as flutes, ribs or secondary lumens to prevent the balloon being
15 sucked into the bushing during deflation of the balloon. The neck portion of the balloon is preferably adapted for sealing connection with the bushing. The bushing preferably has a taper adapting the relatively large diameter of the neck of the balloon to the relatively small diameter of an hydraulic or pneumatic fluid line connecting the balloon to a power source. This taper is preferably elongated to enhance the flexibility of the bushing along
20 its central axis.

In a fifth aspect, the present invention provides an actuator for a heart assist device, the actuator including:

a flexible inflatable balloon having a neck portion connected at one end to a bulbous body portion having a first and a second side; and

25 a substantially inelastic shroud or wrap having a flared portion that extends over the adjacent first side of the balloon bulbous portion,

wherein, during deflation, the second side of the bulbous body portion is able to be drawn against the first side of the bulbous body portion.

The shroud or wrap preferably supports the first side of the balloon bulbous portion against substantial movement whilst the second side of the balloon bulbous portion is free to move during inflation and deflation.
30

In a sixth aspect, the present invention provides a method of providing extra-aortic heart assistance using the actuator of the first or the second or the fifth aspect or the heart assist device according to the third aspect or the balloon of the fourth aspect, the

method including mounting the balloon second body portion adjacent the exterior of an arterial vessel.

5 In a seventh aspect, the present invention provides a method of providing intra-aortic heart assistance using the actuator according to the first or the second or the fifth aspect or the heart assist device according to the third aspect, the method including resecting a portion of an arterial vessel and mounting the balloon with the balloon second body portion sealingly replacing the resected arterial portion.

Brief Description of the Drawings

10 Preferred embodiments of the invention will now be described, by way of examples only, with reference to the accompanying drawings in which:

Fig. 1 is an exploded perspective view of a first embodiment of an actuator according to the invention;

Fig. 2 is a assembled, partial cut away, perspective view of the actuator shown in Fig. 1;

15 Fig. 3 is an assembled, cross sectional view of the actuator shown in Fig. 1 along the line 3-3;

Fig. 4 is a assembled, cross sectional view of the actuator shown in Fig. 1 along the line 4-4;

20 Fig. 5 is a cross sectional view of the second embodiment of an actuator according to the invention along the line 5-5;

Fig. 6 is an underside view of the bushing used in the actuator shown in Fig. 5;

Fig. 7 is a cut away perspective view of a balloon for a third embodiment of an actuator according to the invention;

Fig. 8 is a top view of the balloon shown in Fig. 7;

25 Fig. 9 is a cut away side view view of a fourth embodiment of an actuator according to the invention;

Fig. 10 is a perspective view of the actuator shown in Fig. 9; and

Fig. 11 is a front view of the actuator shown in Fig. 9.

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Detailed Description of the Preferred Embodiments

Fig.1 shows an exploded perspective view of an actuator 10 according to a first embodiment of the present invention, which is sized for pediatric use. The actuator 10

has a flexible, inflatable balloon 12, an inelastic shroud 14 and a relatively rigid bushing 16.

5 The balloon 12 is formed from Polyurethane by mandrel dipping. The balloon 12 has a narrower neck portion 18 which is connected by a flared part 20 to a wider first body portion 22. A flexure region 24, which extends generally around the exterior of the balloon 12 at its widest part connects a second body portion 26 (see Figs. 2 to 4) to the first body portion 22.

10 When viewed in plan, the first and second body portions are generally elliptical in shape and have a maximum width and length of about 31-35mm and 55-60mm respectively. The balloon neck portion has a diameter of approximately 10-14mm at its distal end 18a and, at its proximal end 18b, it is elliptical in shape with dimensions of approximately 40-50mm in the long axis and 20-30mm in the short axis of the balloon 12, and with a converging taper therebetween.

15 The shroud 14 is formed, by mandrel dipping, from a material substantially equivalent to the material used for the balloon, such as a polurethane or a polyurethane-polysiloxane block co-polymer. The shroud 14 has a narrower neck portion 28 which is joined to a wider body portion 30 by a flared part 32. The shroud body portion 30 is also generally elliptical in shape when viewed in plan and has a larger peripheral extent (ie extends further in all directions) than the balloon body portions 22 and 26 and flexure region 24. More particularly, the shroud body portion 30 has a length (along the long axis of the balloon 12) of 60-100mm and a minimum width of (across the short axis of the balloon 12) of 33mm. The shroud neck portion 28 is sized to be a snug sealing fit over the exterior of the balloon neck portion 18.

25 The bushing 16 is formed, by injection moulding, from a flexible plastic such as Polyurethane. The bushing 16 has a hollow bore 36 which is adapted for sealing connection with a fluid line from a motive power source such as a fluid pump (not shown). Suitable pumps are disclosed in the Applicant's International PCT Patent Application No. PCT/AU02/00974 entitled "A fluid pressure generating means", the contents of which are hereby incorporated by cross reference. The bushing 16 also has a relatively more tapered distal part 38 and a relatively less tapered proximal part 40. The proximal part 40 is sized to be a snug sealing fit within the interior of the balloon neck portion 18.

30 Fig. 2 shows the device 10 after assembly. The assembly comprises initially stretching the neck portion 18 of the balloon 12 so that the proximal part 40 of the

bushing 16 can be inserted therein. The balloon 12 is retained adjacent the bushing 16 by the shroud 14 being forced past the distal part 38 of the bushing 16 until it is a snug sealing fit on the exterior of the balloon neck portion 18 as shown. The bushing proximal part 40, the balloon neck portion 18 and the shroud neck portion 28 all have a common taper angle. The components are also bonded together with a suitable adhesive in order to ensure an effective seal therebetween.

The operation of the device 10 will now be described by with reference to Figs. 3 and 4. Fig. 3 is a cross-sectional (anterior) view along the longitudinal direction of the aorta. Fig. 4 is a partial cross-sectional view orientated at 90 degrees from that of Fig. 3.

For extra-aortic heart assistance, the device 10 is placed with the balloon second portion 26 adjacent the exterior of an arterial vessel, most preferably the outer part of the ascending aorta (not shown). A flexible, relatively inelastic wrap is placed over the shroud 30 and around the aorta in order to retain the device 10 in place. Wraps are well known in the art and thus will not be described in further detail. The wrap can also be used in place of the shroud.

In use, fluid is cyclically driven to and from the balloon 12, via the bushing bore 36, to cyclically inflate and deflate the balloon 12. The inflated balloon 12 is shown in solid line in Fig. 3. The inflated balloon 12 compresses the aorta and thus assist in blood displacement during diastole. When the balloon 12 is deflated it retracts to the position shown in phantom line, which allows the aorta to return to its natural shape during systole.

As Figs. 3 and 4 show, when the balloon 12 is inflated the shroud 14 restrains the balloon first portion 22, up to and including the part adjacent the flexure region 24, against outward displacement past a predetermined limit. That limit being defined by the shape of the shroud body portion 30. However, the shroud 14 does not restrain the inward displacement of the balloon first portion 22, particularly that part at or near the flexure region 24, during deflation. This allows the balloon 12 to always retain a relatively large radius of curvature (e.g. 1.0mm) adjacent the flexure region 24, which is the part of the balloon 12 that undergoes the most deformation. This advantageously minimises stress concentration in the flexure region 24, which results in a much more reliable and longer lasting balloon 18.

This is in contrast to the balloons shown in the two prior art documents mentioned previously which are restrained at a region equivalent to the flexure region for both inward and outward displacement. These balloons undergo a movement akin to

pivoting or bending at their free edge. This results in high levels of stress concentration, and associated high levels of failure, in those balloons.

5 The device 10 is also simpler, and thus cheaper, to assemble and manufacture than the prior art devices as the bushing 16 only engages with the balloon 12 in the region of their respective neck portions 40, 18, as opposed to positioning the bushing (or shell) more fully within the body portions of the balloon.

Figs. 5 and 6 show a second embodiment of blood displacing device 50 according to the invention. The device 50 is similar to the first embodiment and like reference numerals are used to indicate like features.

10 The major difference between the two embodiments is that the bushing 16 in the device 50 includes a series of internal projections 52 which serve to stop the balloon 18 being sucked into the bore 36 of the bushing during large amounts of suction/deflation. Such large amounts of suction/deflation can occur during the calibration cycle of some of the pumps suitable for use with the blood displacing device 50.

15 Figs. 7 and 8 show a balloon 60 for a third embodiment of actuator according to the invention. The balloon 60 is sized for adult use is but is otherwise similar to the first embodiment and like reference numerals are used to indicate like features. When viewed in plan, the first and second body portions 24 and 26 are generally elliptical in shape and have a maximum width and length of 32mm and 65mm respectively. The balloon neck
20 portion has a diameter of approximately 10mm at its distal end 18a and approximately 26-44mm (oval in cross-section) at its proximal end 18b and a conical converging taper therebetween.

Figs. 8 to 10 show a fourth embodiment of actuator 70 according to the invention. Like features to earlier embodiments are indicated with like reference
25 numerals. The actuator 70 utilises the balloon 60 shown in Figs. 7 and 8. The bushing 16 of the actuator 70 differs from earlier embodiments in that it is substantially hollow with a central cylindrical part 16a attached at one end to an outer flared conical part 16b. A series of radial webs 16c are provided between the central cylindrical part 16a and the flared conical part 16b. A flexible, relatively inelastic wrap 72 is provided over the
30 balloon 60, which has an opening 72a through which the bushing 16 protrudes.

It will be appreciated by the persons skilled in the art that numerous variations and/or modifications can be made to the invention as shown in the specific embodiment without departing from the spirit or scope of the invention as broadly defined. For example, the blood displacing devices are described above in relation to extra-aortic

counter-pulsation but also suitable for intra aortic counter-pulsation. In the latter the second portion of the balloon replaces a resected portion of arterial vessel, with the opening made in the resected arterial vessel being sealingly connected to the balloon adjacent the flexure region.

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Dated 11 November, 2003
Sunshine Heart Company Pty Ltd
Patent Attorneys for the Applicant
SPRUSON & FERGUSON

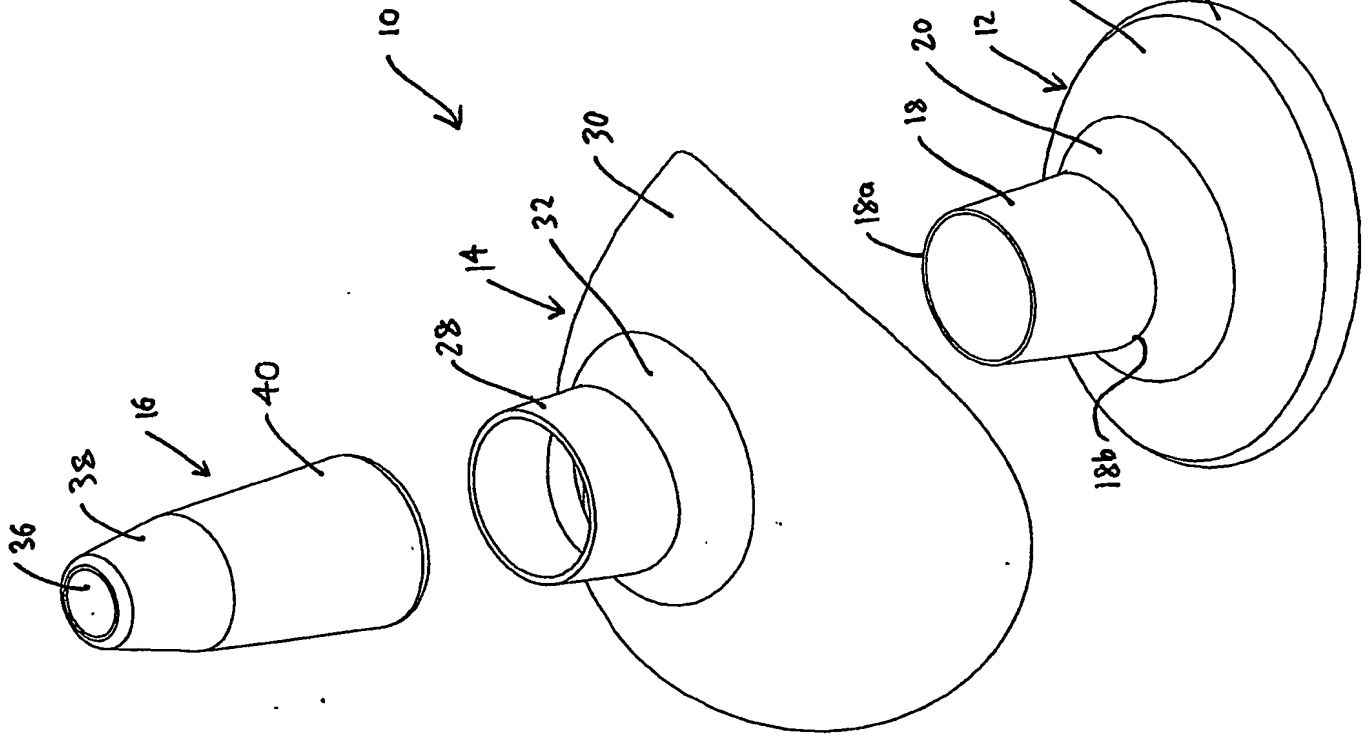
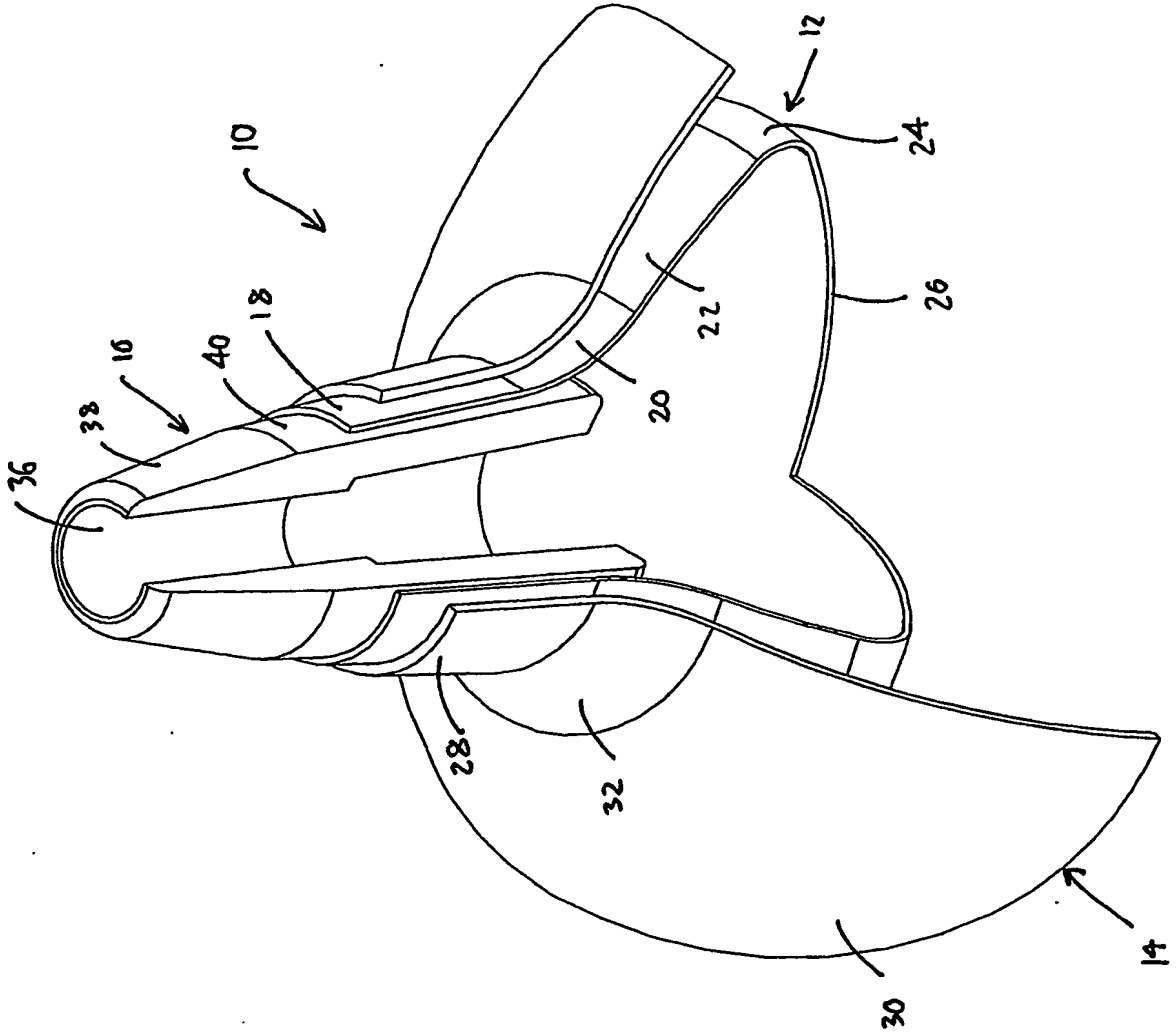
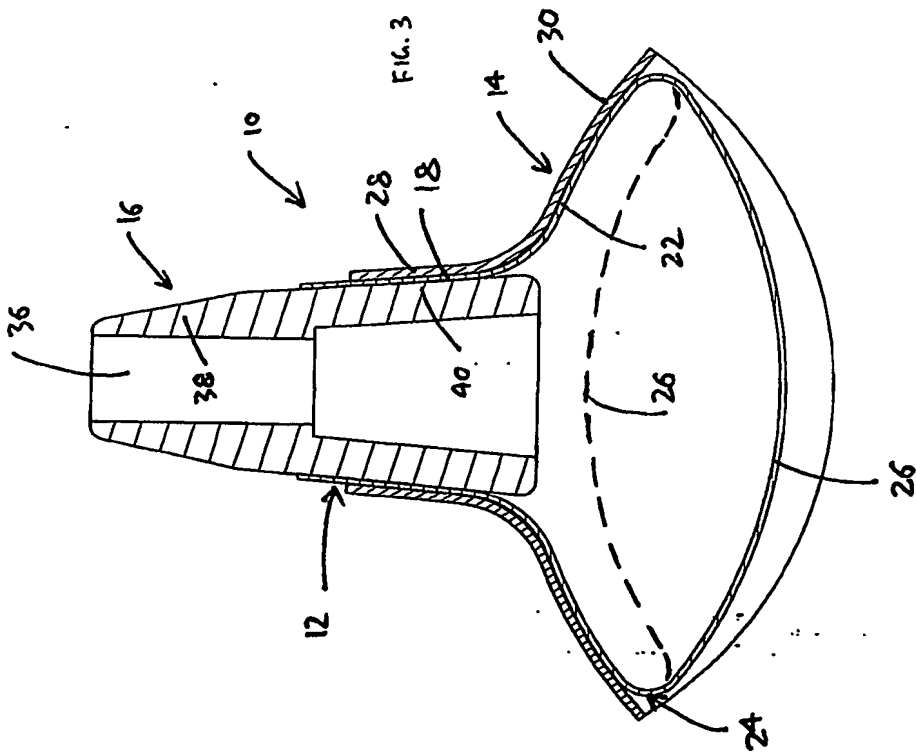
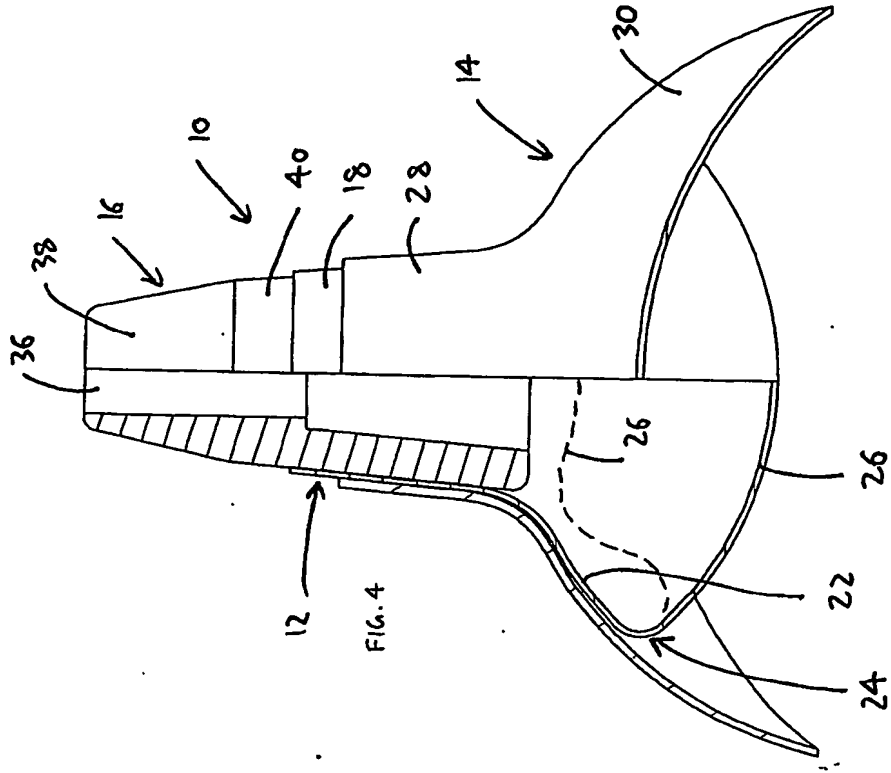
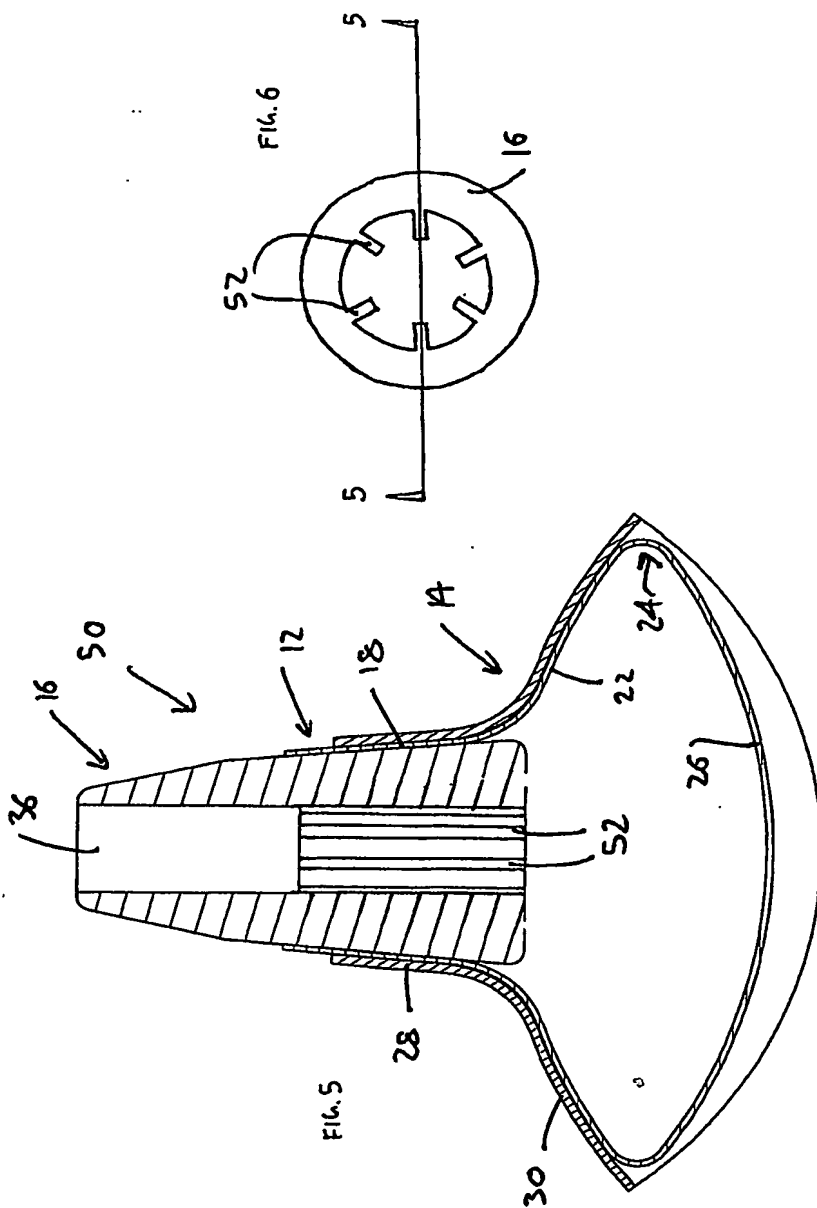
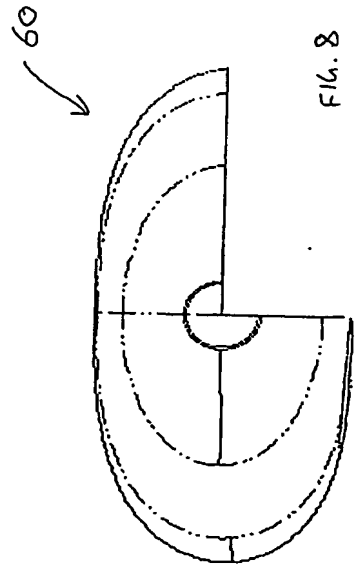
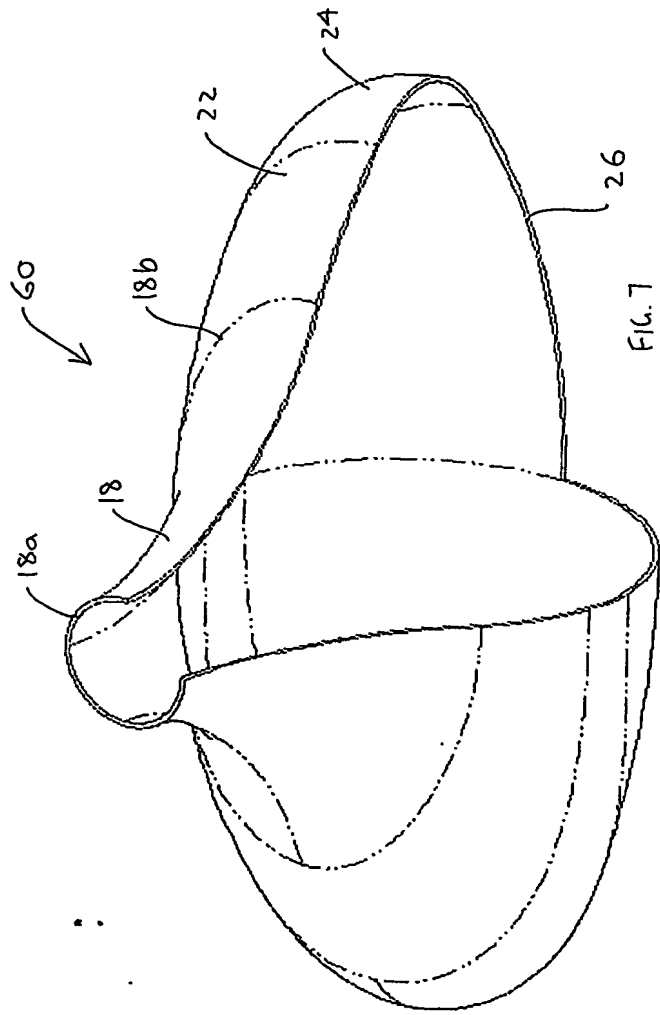


FIG. 2









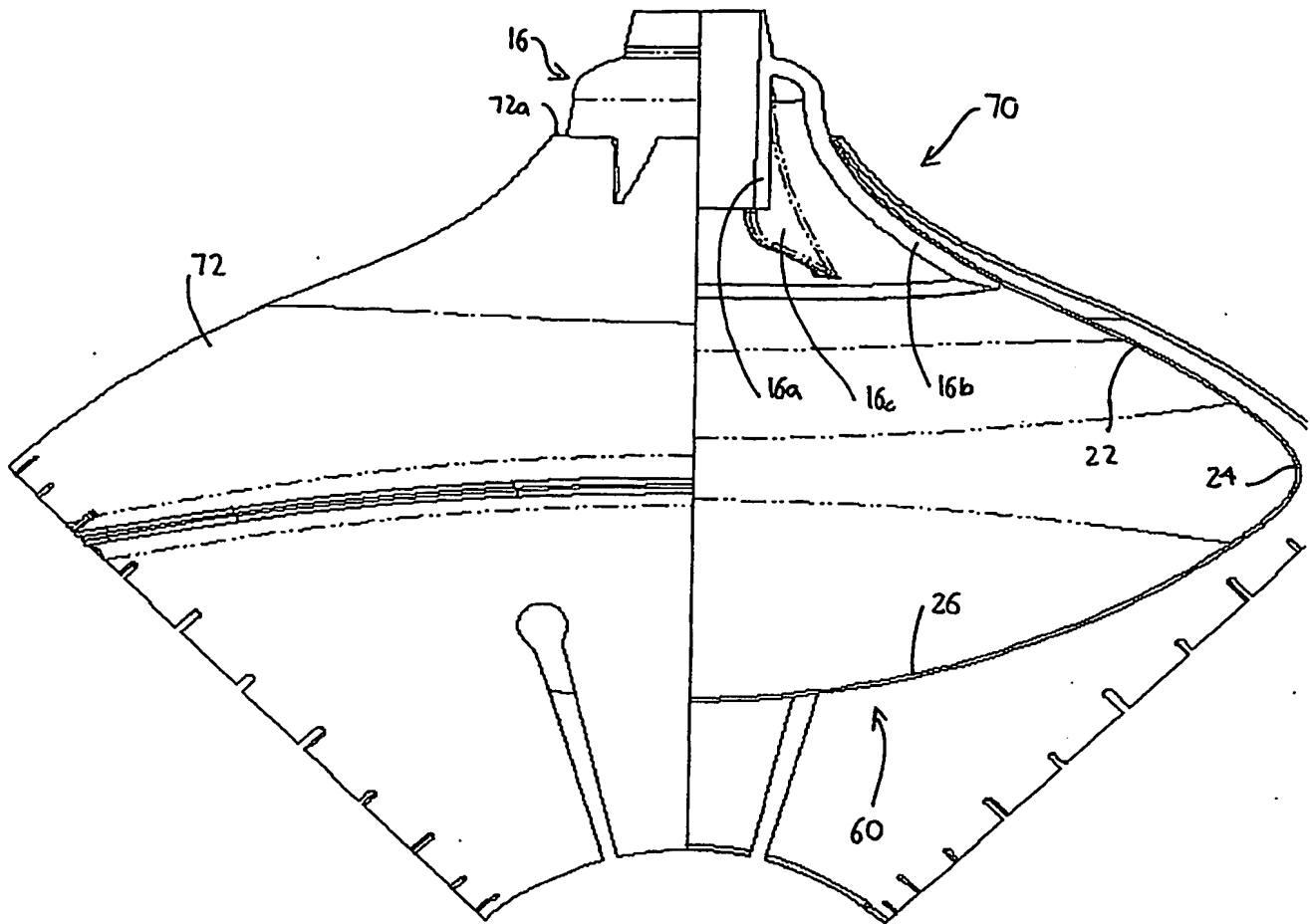


FIG. 9

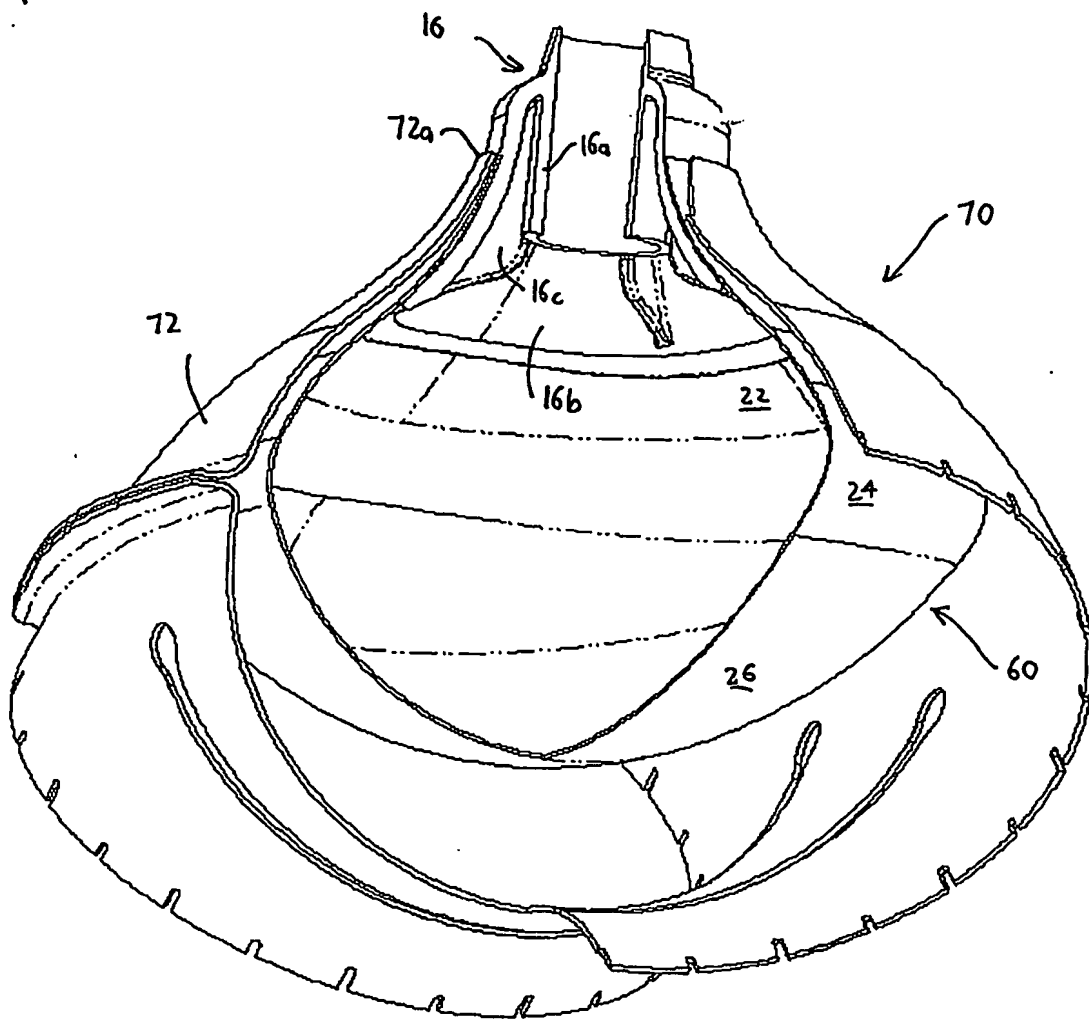


FIG. 10

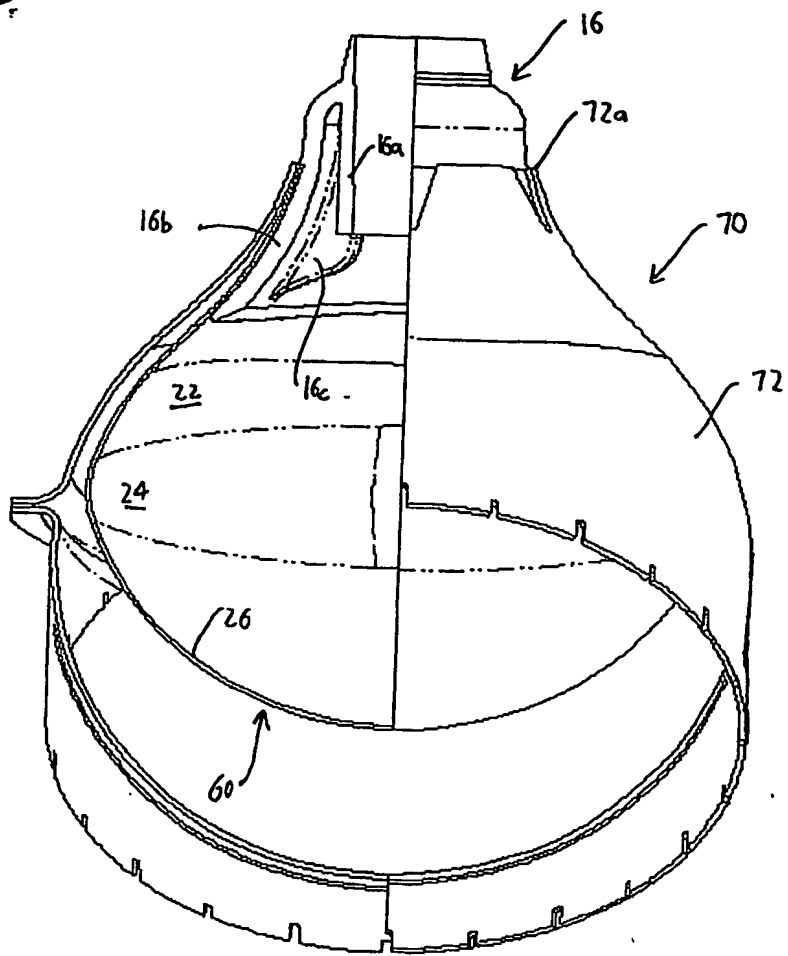


FIG. 11

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